Safety and Health at Work 12 (2021) 511-516

Contents lists available at ScienceDirect

Safety and Health at Work

journal homepage: www.e-shaw.net



Predicting Ability of Dynamic Balance in Construction Workers Based on Demographic Information and Anthropometric Dimensions



Fateme H. Abdolahi¹, Ali S. Variani², Sakineh Varmazyar^{3,*}

¹ MSc of Occupational Health Engineering, Faculty of Health, Student Research Committee, Qazvin University of Medical Sciences, Qazvin, Iran

² Department of Occupational Health Engineering, Faculty of Health, Qazvin University of Medical Sciences, Qazvin, Iran

³ Department of Occupational Health Engineering, Social Determinants Health Research Center, Research Institute for Prevention of Non-Communicable

Diseases, Faculty of Health, Qazvin University of Medical Sciences, Qazvin, Iran

ARTICLE INFO

Article history: Received 19 February 2021 Received in revised form 14 July 2021 Accepted 14 July 2021 Available online 21 July 2021

Keywords: Anthropometry Construction Dynamic Worker Balance

OSHR

Original article

ABSTRACT

Background: Difficulties in walking and balance are risk factors for falling. This study aimed to predict dynamic balance based on demographic information and anthropometric dimensions in construction workers.

Methods: This descriptive-analytical study was conducted on 114 construction workers in 2020. First, the construction workers were asked to complete the demographic questionnaire determined in order to be included in the study. Then anthropometric dimensions were measured. The dynamic balance of participants was also assessed using the Y Balance test kit. Dynamic balance prediction was performed based on demographic information and anthropometric dimensions using multiple linear regression with SPSS software version 25.

Results: The highest average normalized reach distances of YBT were in the anterior direction and were $92.23 \pm 12.43\%$ and $92.28 \pm 9.26\%$ for right and left foot, respectively. Both maximal and average normalized composite reach in the YBT in each leg were negatively correlated with leg length and navicular drop and positively correlated with the ratio of sitting height to leg length. In addition, multiple linear regressions showed that age, navicular drop, leg length, and foot surface could predict 23\% of the variance in YBT average normalized composite reach of the right leg, and age, navicular drop, and leg length could predict 21% of that in the left leg among construction workers.

Conclusion: Approximately one-fifth of the variability in the normalized composite reach of dynamic balance reach among construction workers using method YBT can be predicted by variables age, navicular drop, leg length, and foot surface.

© 2021 Occupational Safety and Health Research Institute, Published by Elsevier Korea LLC. This is an open access article under the CC BY-NC-ND license (http://creativecommons.org/licenses/by-nc-nd/4.0/).

1. Introduction

Falling is an important hazard that threatens workers in industrial and occupational processes [1]. Falling has serious, catastrophic, and even fatal complications. In some occupations, especially construction jobs, falling is the main and most important threat to workers [2,3]. Based on the nature of work in the construction industries, which are inherently dangerous, fall accidents are one of the major causes of occupational fatalities, representing 33% of all fatalities in constructions [4]. According to the Occupational Safety and Health Administration report (2019), 21.1% of workers fatalities in private industries occurred in construction, which means one in five deaths in workers was related to construction [5]. There are some situations at construction sites where we cannot eliminate risks even through a fall arrest system which prevents accidents at construction sites [6]. Difficulties in walking and balance are considered risk factors for falling [7]. Balance is a complex motor skill that involves the interaction of several complex systems, including muscular, skeletal, and nervous systems, with the environment [8]. Therefore, numerous risk factors can result in loss of balance incidents on construction sites [9]. Good individual balance ability can be essential for safe and efficient work performance; it may also improve health, modify workability, and reduce the risk of falling [10]. Studies have shown that age, height, weight, foot shape, body composition, and level of activity, and health can affect balance ability, as well as type and severity of injury [11,12].

* Corresponding author. Qazvin University of Medical Sciences, Shahid Bahonar Boulevard, Qazvin, 34199-15315, Iran. *E-mail address:* Svarmazyar@qums.ac.ir (S. Varmazyar).

^{2093-7911/\$ -} see front matter © 2021 Occupational Safety and Health Research Institute, Published by Elsevier Korea LLC. This is an open access article under the CC BY-NC-ND license (http://creativecommons.org/licenses/by-nc-nd/4.0/). https://doi.org/10.1016/j.shaw.2021.07.009

Nakallio reported that balance abilities have a negative correlation with age in firefighters [13]. Moein et al. reported that there were significant mild correlations between the lower leg length and body mass index with dynamic balance, and no significant relationships were found between other anthropometric features with dynamic balance in sedentary female college students [14]. Meyvaci et al. found significant effects of different foot and body parameters on functional balance performances in young male adults [15]. Lencioni et al. reported that anthropometry parameters like sex, age, body mass, and height, mainly in the frontal plane, have a significant effect on dynamic balance [16].

Body stability can be analyzed by examining dynamic and postural stability [17]. The Y Balance Test, a modified version of the Star Excursion Balance Test (SEBT), is used to assess the risk of falling in various populations and identifying any deficiency of functional movement, dynamic balance performance, and stability [18,19]. The YBT examines the distance a subject can extend the Center of Gravity (COG) over the Base of Support (BOS) to quantify boundaries of the limit of sway [20].

There is little information on the effect of individual and anthropometric characteristics on balance ability in construction workers. Therefore, this study was conducted to monitor the postural control of construction workers and investigate associations between dynamic balance abilities with demographic information and anthropometric indices.

2. Methods

2.1. Participants

This is a descriptive-analytical study conducted in 2020. One hundred and forty construction workers were asked to complete the injury history questionnaire before taking part in the study. The inclusion criteria were lack of neuromuscular and musculoskeletal diseases, including stroke, Parkinson's disease, ataxia, multiple sclerosis, symptoms of unsteadiness, dizziness or vertigo, impaired sensory function, uncorrected visual problems, ear infection, and no history of surgery on the lower limbs, and trunk in the last year. Subjects also stated that they were not taking any medication such as sedatives, hypnotics, anxiolytics, antihypertensive drugs, antipsychotics, anticholinergics, and antidepressants, and all individuals gave their personal written informed consent to participate in this study. Then 26 of them were eliminated because they did not have the required qualifications to enter the study. As a result, 114 male construction workers with normal BMI (18.5–24.9 kg/m²) [21] participated in the study.

2.2. Demographic questionnaire and inclusion criteria

A demographic questionnaire was used to collect personal and occupational information, including age, height, weight, and work experience. The final questions of the questionnaire were related to factors related to entering the study.

2.3. Measurements of anthropometry dimensions

The anthropometry dimensions were measured using a measuring tape, anthropometer device, Marcal digital caliper, and Omron digital scale, including age, weight, height, sitting height, leg length, foot length, foot surface area (FSA = 1.043 \times footlength \times ball-girth) [22], ankle width, foot breadth, heel width, ankle circumference, thigh circumference, hip breadth [23,24], and navicular drop was measured using Brody Method [25,26]. For measuring the navicular drop, participants were asked to sit in a relaxed position -hip and knee flexed at 90 degrees on a chair and place their barefoot on a firm supporting surface or on a box with 10 cm height (floor or step). The furthest protruding part of the medial navicular tubercle was marked, and then the distance from the ground to the marked navicular tubercle was measured with a plastic ruler. After that, participants were asked to stand with equal weight on both feet. The new distance was also measured. Afterward, the navicular drop was obtained by comparing measured values between the sitting and standing positions. Each measurement was conducted three times. Then, the mean was calculated.

Then, participants were classified into normal (within a range of 5 to 9 mm), flat arch (More and equal than 10 mm), and high arch (less and equal than 4 mm) foot groups based on the rate of the navicular drop [25].

2.4. Y balance test (YBT)

YBT was performed using the Y balance test kit. Participants stood with one leg on the center of the Y board, and the other leg touched down lightly just behind the plate. They reached out in the desired direction with the free leg and pushed the reach indicator

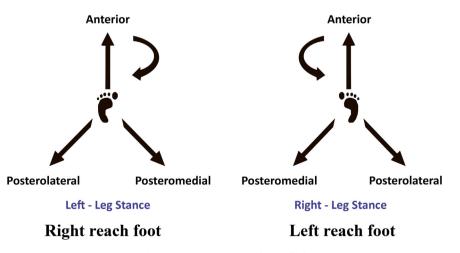


Fig. 1. Reach directions tasks for YBT [31].

Table 1

Quantitative demographic, occupational, and anthropometry information of study participants (n=114)

Quantitative information					
Variables	$\text{Mean}\pm\text{SD}$				
Age (years)	37.79 ± 9.82				
Height (cm)	176.13 ± 6.29				
Weight (kg)	73.28 ± 8.09				
Work experience (years)	12.85 ± 8.29				
Leg length (cm)	92.11 ± 4.33				
Sitting Height Leg Length	1.01 ± 0.04				
Foot Length (cm)	28.01 ± 1.83				
Foot Surface (cm ²)	741.81 ± 72.72				
Ankle Width (cm)	$\textbf{6.6} \pm \textbf{0.66}$				
Foot Width (cm)	9.58 ± 0.52				
Heel Width (cm)	6.75 ± 0.68				
Ankle Circumference (cm)	25.29 ± 1.96				
Thigh Circumference (cm)	5.39 ± 53.84				
Hip Breadth (cm)	34.10 ± 1.92				
Navicular Drop (mm)	0.95 ± 0.43				
SD: Standard Deviation.					

as far as possible while maintaining balance. After the operation was completed in this procedure, the free foot had to be returned to the starting position. Participants were able to choose the leg to be used as the stance leg first. Three attempts were made in each anterior, posteromedial, and posterolateral direction. Participants with the right stand foot (left reach foot) performed the test in a counterclockwise direction, and those with the left stand foot (right reach foot) performed the test in a clockwise direction (Fig. 1). Participants were justified that they could not perform in following the touching down of the free leg during movement to keep balance or putting their foot on top of the reach indicator to gain support, kicking out the indicator, and crossing the starting line with their stance foot. The maximal and average reach (a distance read from the demarcated line at the proximal edge of the reach indicator) were recorded after three successful trials in each direction. Then the normalized value was calculated for both legs as composite reach and the maximal reach and average of three reach trials divided by leg length, then multiplied by 100% [18,27-30].

2.5. Statistical analysis

Descriptive results of YBT (n = 114)

Table 2

Descriptive statistics were used to report demographic and anthropometric information. Then the Kolmogorov-Smirnov test (K-S) was used to test normality of the data. Pearson correlation coefficient was used to investigate the relationship between dependent and independent variables. A backward stepwise multiple linear regression analysis was used to determine if anthropometric parameters could predict dynamic balance. All analyzes were performed by SPSS software version 25.

3. Results

The results showed that the mean and standard deviation of age were 37.79 ± 9.82 years. Table 1 represents the characteristics of individuals who participated in the study.

Based on the navicular drop test measurements, the medial longitudinal arch was classified into three groups in construction workers. So that 7% of the participants were in the high arch (\leq 4mm) category, 43.9% in the normal (5–9 mm) category, and 49.1 in the flat arch (\geq 10 mm) category.

The means and standard deviations of the maximal and average normalized reach of three trials in each direction of both limbs for YBT are shown in Table 2. On average, subjects showed $86.42 \pm 9.28\%$ normalized composite reach for right, and $85.93 \pm 9.75\%$ normalized composite reach for left.

Evaluation of normal distribution of dependent variable based on the Kolmogorov-Smirnov test showed that the YBT data have a normal distribution ($P \ge 0.05$).

A significant negative correlation was found between anthropometric dimensions of age, height, weight, leg length, foot length, and navicular drop with right average and maximal normalized composite reach. There was also a significant negative correlation between leg length and navicular drop with the average and maximal normalized composite reach of left the leg. Other relationships were shown in Table 3.

The Multiple Linear Regression (Backward Elimination Technique) was calculated to predict the Average Normalized Composite Reach of the Right leg (ANCR_R) of YBT based on demographic variables and anthropometric dimensions. The Multiple Linear Regression analyses showed that ANCR_R was significantly associated with age, navicular drop, leg length, and foot surface (F (4,109) = 9.542, p < 0.000), R² of 0.259, and Adjusted R² of 0.232, which indicated that the predictor the model was able to predict 23.2% of the ANCR_R. B values were used for the regression equation to predict the average normalized composite reach of the right and left leg base on the reference [32] (Table 4).

Multiple Linear Regression (Backward Elimination Technique) was used to predict Average Normalized Composite Reach of left leg (ANCR_L) of YBT based on demographic variables and anthropometric dimensions. The Multiple Linear Regression analyses showed that ANCR_L was significantly associated with age, leg length, and navicular drop (F (3,110) = 11.325, p < 0.000), R² of 0.236, and Adjusted R² of 0.215, which indicated the predictor model was able to predict for 21.5% of the ANCR_L (Table 5).

Lower extremity	Direction		Normalized reach (%)					
		Maxima	Maximal reach		Average reach of three trials			
		Mean \pm SD	95% CI	Mean \pm SD	95% CI			
Right	Anterior (A) Posteromedial (PM) Posterolateral (PL) Composite	$\begin{array}{c} 94.33 \pm 8.71 \\ 84.18 \pm 13.21 \\ 83.87 \pm 11.51 \\ 87.46 \pm 9.56 \end{array}$	92.71, 95.95 81.72, 86.63 81.74, 86.01 85.69, 89.23	$\begin{array}{c}92.23\pm 12.43\\83.56\pm 11.60\\82.58\pm 11.52\\86.42\pm 9.28\end{array}$	89.93, 94.54 81.41, 85.72 80.44, 84.72 84.70, 88.14			
Left	Anterior (A) Posteromedial (PM) Posterolateral (PL) Composite	$\begin{array}{c} 93.53 \pm 9.18 \\ 85.22 \pm 11.67 \\ 82.64 \pm 10.89 \\ 87.13 \pm 9.66 \end{array}$	91.3, 95.24 83.05, 87.38 80.62, 84.66 85.34, 88.92	$\begin{array}{c}92.28\pm 9.26\\83.94\pm 11.81\\81.57\pm 11.05\\85.93\pm 9.75\end{array}$	90.57,94.00 81.74, 86.13 79.52, 83.62 84.12, 87.74			

Table 3

Correlations of demographic and anthropometric dimensions with YBT-based average and maximal normalized composite reach

Variables		Right				Left			
	Average normalized composite reach		Maximal normalized composite reach			Average normalized composite reach		Maximal normalized composite reach	
	r	<i>P-</i> value	r	<i>P-</i> value	r	<i>P-</i> value	r	<i>P-</i> value	
Age	-0.19	0.03	-0.17	<0.01	-0.13	0.14	-0.12	0.20	
Height	-0.20	0.02	-0.22	0.03	-0.15	0.09	-0.17	0.05	
Weight	-0.17	0.05	-0.19	0.03	-0.12	0.10	-0.15	0.12	
Leg length	-0.37	<0.01	-0.40	< 0.01	-0.40	< 0.01	-0.41	<0.01	
Sitting Height Leg Length	0.27	<0.01	0.27	<0.01	0.27	<0.01	0.26	<0.01	
Foot Length	-0.25	<0.01	-0.22	< 0.01	-0.13	0.16	-0.16	0.15	
Foot Surface	0.20	0.03	0.17	0.05	0.08	0.37	0.08	0.34	
Ankle Width	-0.12	0.18	-0.14	0.13	-0.07	0.42	-0.07	0.42	
Foot Width	-0.10	0.24	-0.09	0.31	-0.10	0.26	-0.09	0.30	
Heel Width	0.05	0.56	0.05	0.57	0.00	0.99	0.00	0.92	
Ankle Circumference	0.08	0.35	0.15	0.22	0.07	0.46	0.07	0.45	
Thigh Circumference	0.09	0.30	0.07	0.45	0.16	0.07	0.16	0.08	
Hip Breadth	-0.13	0.14	-0.14	0.11	-0.04	0.65	-0.04	0.61	
Navicular Drop	-0.25	<0.01	-0.24	<0.01	-0.24	<0.01	-0.24	<0.01	

4. Discussion

The objective of this study was to investigate demographic and anthropometric predictors of the ability of dynamic balance in construction workers and to determine which anthropometric dimension has a greater role in predicting normal composite reach among construction workers.

In the YBT test, more reach in three directions indicates better equilibrium [18]. A study of dynamic balance by YBT showed that the highest average normalized reach of right and left foot is in the anterior, posteromedial, and posterolateral directions, respectively. The average combined reach distance of three directions of the right foot of construction workers is more than the left foot.

The results of this study showed that there was a statistically significant negative correlation between age and right composite reach. This means that there would be less dynamic balance in construction workers as they get older. The results also showed that about 0.238 of the composite score of the right leg and about 0.186 of the composite score of the left leg of YBT would be reduced by increasing age. In line with the present study, Nakallio [13] indicated that balance abilities in younger firefighters are better than those aged 50 and older. Robertson et al. [33] reported a significant reduction in Tandem walk eyes open capacity in participants aged 20–80 years. Norheim et al. [34] showed that dynamic balance and lower extremity function were negatively associated with age in manual workers aged 51–72 years. Regarding the effect of age on balance, it seems that older people lose balance function through loss of sensory elements, ability to integrate information and issue

motor commands and lose musculoskeletal function, destroys cells in the vestibular system, affecting older ability to correct our position [35]. Also, in old age, several conditions occur at the same time, such as hearing loss, cataracts, and refractive errors, back and neck pain, and osteoarthritis [36].

As shown, there was a statistically significant negative correlation between height and right composite reach and maximal left composite reach. This means that the taller a person is, the lower the dynamic balance is. Alonso et al. pointed out that height was the most influential anthropometric variable on postural balance [11], which is consistent with the results of other studies [37,38]. They reported that shorter body height explains the better performance of balance ability. However, our observations were not compatible with those of Neji et al. [39] and Tabrizi et al. [40]. They showed that height has a significant positive correlation with dynamic balance. The observed differences may have occurred because of some differences due to the age, body compositions of the subjects, methods, and physical conditions.

In this study, there was a statistically significant difference between weight and right composite reach. This means that a decrease in dynamic balance is strongly correlated to an increase in body weight. This is in line with the result of previous studies [40– 43]. These studies indicated that increased body weight affects balance function, and it can lead to poorer balance control. Bodyweight correlated with the mean speed of the center of pressure [43]. This suggests that, when submitted to daily postural stresses and perturbations, obese persons, particularly those with an abnormal distribution of body fat in the abdominal area, may be at

Table 4

Prediction of the average normalized composite reach of the right leg (ANCR_R) obtained from demographic information and anthropometric dimensions based on multiple linear regression test

	Sig	F	Adjusted R ²	R ²	B (unstandardized coefficient)	Beta (standardized coefficient)	t
(Constant)	0.00	_	_	_	182.70	_	10.21
Age	0.00	—	_	_	0.238-	-0.25	-3.03
Leg length	0.00	—	_	—	-0.760	-0.35	-4.17
Navicular drop	0.02	_	_	_	-0.397	-0.18	-2.25
Foot surface	0.09	—	_	—	0.018	0.14	1.69
Total	0.00	9.542	0.232	0.259	—	—	_

Table 5

Prediction of the average normalized composite reach of left leg (NACR_L) obtained from demographic information and anthropometric dimensions based on multiple linear regression test

	Sig	F	Adjusted R ²	R ²	B (unstandardized coefficient)	Beta (standardized coefficient)	t
(Constant)	0.00	_	—	_	180.16	_	9.95
Age	0.00	—	—	—	0.186-	-0.187	-2.22
Leg length	0.02	—	—	—	-0.903	-0.401	-4.72
Navicular drop	0.02	—	—	—	-0.422	-0.190	-2.26
Total	0.00	11.32	0.215	0.236	_	-	_

higher risk of falling than lightweight individuals because they have to generate ankle torque more rapidly and with a much higher rate of torque development to recover balance [44,45].

The results of this study indicated that there was a statistically significant negative correlation between leg length with right and left normalized composite reach. According to regression analysis, leg length explained about 0.760 normalized composite reach of the right leg and about 0.903 of normal composite reach of the left leg of YBT. That shows aone-centimeter increase in leg length predicting a drop in normalized composite reach of 0.76 and 0.903 percentage points for the right and left legs, respectively, which is consistent with the results of a study conducted by Ferreira et al. [12]; they indicated that the greater the lower limb length, the worse the directional balance control if the female group and inconsistent with the results of studies conducted by Gribble et al. [46].

Also, it pointed out that there was a significant positive correlation between the ratio of sitting height to leg length with right and left composite reach distance. This means that individuals with higher sitting height showed better performance in the dynamic balance test than those who had longer leg length.

It was obtained that there was a significant negative correlation between foot length and right composite reach. The results of current are consistent with previous findings of the study by Babayigit [47] that showed a negative correlation between dynamic balance and foot length. Ferreira et al. [12] showed that foot size had a weak effect on postural balance control in male and female groups. Birinci and Demirbas [48] reported that foot length was not associated with dynamic balance on bipedal stance. The observed differences may have occurred because of the differences in the physical conditions, methodology, the body compositions of the subjects, and individuals who did not have the same age.

As it was observed, there was a significant positive correlation between foot surface and right composite reach distance. This means that decreased foot surface resulted in a negative effect on participants' dynamic balance. It could be explained by the fact that increased foot surface area increases the base of support, thereby making the individual more stable [12,49]. Ferreira et al. indicated that females with larger foot sizes have faster reaction times and in the male group, the narrower the foot, the worse the control of balance, which maintains that the increase in the base of support size improves postural balance.

A significant negative correlation was obtained between navicular drop and composite reach distance of YBT. It was also found that about 0.397 of the composite score of the right leg and about 0.422 of the composite score of the left leg of YBT would be reduced by increasing navicular drop. This result is consistent with the results of a study conducted by Sachini et al. [50]. They reported that differences in the foot arch, especially the flat arch, could cause weakness and decline in balance ability. However, Birinci found that navicular height was not associated with dynamic and static balance [48]. Kim reported that static balance is affected in flat feet individuals but not dynamic balance [51]. These results, taken together, suggest that a flat arch of longitudinal affects dynamic balance. Our results also suggest that when construction workers have normal levels of the arch, they show better balance ability.

5. Conclusions

Fifty-six and one-tenth percent of construction workers did not have a normal medial longitudinal arch. Among the participants, the average normalized composite reach of the right leg was 86.42%, which was higher than the average normalized composite reach of the left leg. The maximal normalized reach in both legs in the anterior direction was higher than in other directions. The multiple linear regression revealed that age, navicular drop, leg length, and foot surface could predict 23% of the variance of the average normalized composite reach of the right leg, that among them, leg length plays the most important role. Age, navicular drop, and leg length with 21% are the predictor variables of average normalized composite reach of the left leg, which leg length had the greatest effect. As a result, among the predictors, leg length and the Navicular drop or medial longitudinal arch height of the foot was the anthropometric dimension that had the most effect on the average normalized composite reach in both feet, respectively.

Funding

This research did not receive any specific funding.

Conflicts of interest

The authors declare they have no conflict of interest.

Acknowledgments

The authors would like to express their gratitude to Technical and Civil Deputy of Qazvin Municipality for their generous financial support and sincere cooperation in the data collection process. It should be noted that this article is taken from the thesis approved by the Research Assistant of Qazvin University of Medical Sciences under IR.QUMS.REC.1398.062.

References

- Mihić M. Classification of construction hazards for a universal hazard identification methodology. J Civil Eng Manage 2020;26(2):147–59. <u>https://doi.org/</u> 10.3846/jcem.2020.11932.
- [2] Lette A, Ambelu A, Getahun T, Mekonen S. A survey of work-related injuries among building construction workers in southwestern Ethiopia. Int J Ind Ergon 2018;68:57–64. <u>https://doi.org/10.1016/j.ergon.2018.06.010</u>.
 [3] Sadeghi H, Mohandes SR, Hosseini MR, Banihashemi S, Mahdiyar A,
- [3] Sadeghi H, Mohandes SR, Hossenn MR, Banihashemi S, Mahdiyar A, Abdullah A. Developing an ensemble predictive safety risk assessment model: case of Malaysian construction projects. Int J Environ Res Publ Health 2020;17(22):8395. <u>https://doi.org/10.3390/ijerph17228395</u>.
- [4] Yang K, Jebelli H, Ahn C, Vuran M. Threshold-based approach to detect nearmiss falls of iron workers using inertial measurement units. Comput Civil Eng 2015;2015:148–55. <u>https://doi.org/10.1061/9780784479247.019</u>.
- [5] Alomari K, Gambatese J, Nnaji C, Tymvios N. Impact of risk factors on construction worker safety: a delphi rating study based on field worker perspective. Arab J Sci Eng 2020;45(10):8041–80451.. https://10.1007/ s13369-020-04591-7.
- [6] Sanni-Anibire MO, Mahmoud AS, Hassanain MA, Salami BA. A risk assessment approach for enhancing construction safety performance. Saf Sci 2020;121: 15–29. <u>https://doi.org/10.1016/j.ssci.2019.08.044</u>.
- [7] Cuevas-Trisan R. Balance problems and fall risks in the elderly. Phys Med Rehabil Clin N Am 2017;28(4):727–37. <u>https://doi.org/10.1016/</u> j.pmr.2017.06.006.
- [8] National S, Conditioning A, Miller T. In: Edition F, editor. NSCA's guide to tests and assessments. Champaign, IL: Human Kinetics; 2012.
- [9] Antwi-Afari MF, Li H. Fall risk assessment of construction workers based on biomechanical gait stability parameters using wearable insole pressure

system. Adv Eng Inform 2018;38:683–94. <u>https://doi.org/10.1016/j.aei.2018.10.002</u>.

- [10] Antwi-Afari MF, Li H, Seo J, Wong AYL. Automated detection and classification of construction workers' loss of balance events using wearable insole pressure sensors. Autom Constr 2018;96:189–99. <u>https://doi.org/10.1016/j.autcon.2018.09.010</u>.
- [11] Alonso AC, Luna NMS, Mochizuki L, Barbieri F, Santos S, Greve JMDA. The influence of anthropometric factors on postural balance: the relationship between body composition and posturographic measurements in young adults. Clinics 2012;67(12):1433–14341. <u>https://doi.org/10.6061/clinics/</u> 2012(12)14.
- [12] Ferreira BA, Benetti FA, Luna NM, Brech GC, Bocalini DS, Maifrino LBM, et al. Anthropometric factors and body composition and their relationship with dynamic balance tests. Rev Bras Med 2020;26(5):401-5. <u>https://doi.org/ 10.1590/1517-869220202605190218</u>.
 [13] Nakallio AP. Balance abilities of work ers in physically demanding jobs. Uni-
- [13] Nakallio AP. Balance abilities of work ers in physically demanding jobs. University of Kuopio; 2004.
- [14] Moein E, Movaseghi F. Relationship between some anthropometric indices with dynamic and static balance in sedentary female college students. Turk J Sport Exerc 2016;18(1):45–9. https://doi.org/10.15314/tjse.65406.
- [15] Meyvaci SS, Meyvaci T, Kosif R, Dıramali M, Ankarali H. Effect of foot anthropometric measurements on postural stability. Exp Biomed Res 2020;3(3):176–90. <u>https://doi.org/10.30714/j-ebr.2020361056</u>.
- [16] Lencioni TCI, Rabuffetti M, Cattaneo D, Ferrarin M. Measures of dynamic balance during level walking in healthy adult subjects: relationship with age, anthropometry and spatio-temporal gait parameters. Proc Inst Mech Eng H 2020;234(2):131–40. https://doi.org/10.1177/0954411919889237.
- [17] Liu K, Glutting J, Wikstrom E, Gustavsen G, Royer T, Kaminski TW. Examining the diagnostic accuracy of dynamic postural stability measures in differentiating among ankle instability status. Clin Biomech 2013;28(2):211–7. <u>https:// doi.org/10.1016/j.clinbiomech.2012.11.003</u>.
- [18] Gribble PA, Hertel J, Plisky P. Using the Star Excursion Balance Test to assess dynamic postural-control deficits and outcomes in lower extremity injury: a literature and systematic review. J Athl Train 2012;47(3):339–57. <u>https:// doi.org/10.4085/1062-6050-47.3.08</u>.
- [19] Powden CJ, Dodds TK, Gabriel EH. The reliability of the star excursion balance test and lower quarter Y-balance test in healthy adults: a systematic review. Int J Sports Phys Ther 2019;14(5):683. <u>https://doi.org/10.26603/ijspt20190683</u>.
- [20] Gabriel EH, Powden CJ, Hoch MC. Comparison of the Y-balance test and star excursion balance test: utilization of a discrete event simulation. J Sport Rehabil 2020;1(aop):1–6.
- [21] Umar T, Egbu C, Honnurvali MS, Saidani M, Al-Mutairi M. An assessment of health profile and body pain among construction workers. Proc Inst Civil Engineers - Municipal Engineer 2020;173(3):125–35. <u>https://doi.org/</u> 10.1680/jmuen.18.00019.
- [22] Yu C-Y, Tu H-H. Foot surface area database and estimation formula. Appl Ergon 2009;40(4):767–74. <u>https://doi.org/10.1016/j.apergo.2008.08.004</u>.
- [23] Preedy VR. Handbook of anthropometry: physical measures of human form in health and disease. 2012th ed. Springer Science & Business Media; 2012. 3107 p.
- [24] Pheasant S, Haslegrave CM. Bodyspace: anthropometry, ergonomics and the design of work. CRC press; 2005.
- [25] Razeghi M, Batt ME. Foot type classification: a critical review of current methods. Gait Posture 2002;15(3):282–91. <u>https://doi.org/10.1016/S0966-6362(01)00151-5.</u>
- [26] Zuil-Escobar JC, Martínez-Cepa CB, Martín-Urrialde JA, Gómez-Conesa A. Medial longitudinal arch: accuracy, reliability, and correlation between navicular drop test and footprint parameters. J Manipulat Physiol Ther 2018;41(8):672–9. https://doi.org/10.1016/j.jmpt.2018.04.001.
- [27] Nakagawa TH, dos Santos AF, Lessi GC, Petersen RS, Silva RS. Y-balance test asymmetry and frontal plane knee projection angle during single-leg squat as predictors of patellofemoral pain in male military recruits. Phys Ther Sport 2020. <u>https://doi.org/10.1016/j.ptsp.2020.05.011</u>.
- [28] Coughlan GF, Fullam K, Delahunt E, Gissane C, Caulfield BM. A comparison between performance on selected directions of the star excursion balance test and the Y balance test. J Athl Train 2012;47(4):366–71. <u>https://doi.org/ 10.4085/1062-6050-47.4.03</u>.
- [29] Lai WC, Wang D, Chen JB, Vail J, Rugg CM, Hame SL. Lower quarter Y-balance test scores and lower extremity injury in NCAA division I athletes. Orthop J Sports Med 2017;5(8). <u>https://doi.org/10.1177/2325967117723666</u>. 2325967117723666.

- [30] Alnahdi AH, Alderaa AA, Aldali AZ, Alsobayel H. Reference values for the Y Balance Test and the lower extremity functional scale in young healthy adults. J Phys Ther Sci 2015;27(12):3917–39121. <u>https://doi.org/10.1589/jpts.27.3917</u>.
- [31] Philp F, Telford C, Reid D, McCluskey M. Normative performance values of modified star excursion balance test and limb symmetry in female adolescent footballers. Transl Sports Med 2020;3(4):328–36. <u>https://doi.org/10.1002/ tsm2.146</u>.
- [32] Teo T. Handbook of quantitative methods for educational research. Springer Science & Business Media; 2014.
- [33] Robertson M, Gregory R. Effect of age on dynamic walking balance in a healthy population between the ages of 20 and 80 years. Phys Ther Rehabil 2018;5(1):13. <u>https://doi.org/10.7243/2055-2386-5-13</u>.
- [34] Norheim KL, Samani A, Bønløkke JH, Omland Ø, Madeleine P. On the role of ageing and musculoskeletal pain on dynamic balance in manual workers. J Electromyogr Kinesiol 2020;50:102374. <u>https://doi.org/10.1016/j.jelekin.2019.102374</u>.
- [35] King GW, Abreu EL, Cheng A-L, Chertoff KK, Brotto L, Kelly PJ, et al. A multi-modal assessment of balance in elderly and young adults. Oncotarget 2016;7(12):13297–1329306. <u>https://doi.org/10.18632/oncotarget.7758</u>.
 [36] Antwi-Afari MF, Li H, Edwards DJ, Pärn EA, Seo J, Wong A. Effects of different
- [36] Antwi-Afari MF, Li H, Edwards DJ, Pärn EA, Seo J, Wong A. Effects of different weights and lifting postures on balance control following repetitive lifting tasks in construction workers. Int J Build Pathol Adapt 2017. <u>https://doi.org/ 10.1108/IJBPA-05-2017-0025</u>.
- [37] Greve JMDA, Cuğ M, Dülgeroğlu D, Brech GC, Alonso AC. Relationship between anthropometric factors, gender, and balance under unstable conditions in young adults. Biomed Res Int 2013. <u>https://doi.org/10.1155/2013/850424</u>. 2013.
- [38] Kejonen P, Kauranen K, Vanharanta H. The relationship between anthropometric factors and body-balancing movements in postural balance. Arch Phys Med Rehabil 2003;84(1):17–22. <u>https://doi.org/10.1053/apmr.2003.50058</u>.
- [39] Neji Z, Attia A, Negra Y, Sammoud S, Khemiri A, Petrova LG, et al. Lower Quarter Y Balance Test: reliability and relation to anthropometric parameters. J Phys Educ Sport 2020;20(5):2620-7. <u>https://doi.org/10.7752/jpes.2020.05357</u>.
- [40] Tabrizi HB, Abbasi A, Sarvestani HJ. Comparing the static and dynamic balances and their relationship with the anthropometrical characteristics in the athletes of selected sports. Middle East J Sci Res 2013;15(2):216–21. <u>https:// doi.org/10.5829/idosi.mejsr.2013.15.2.7426</u>.
- [41] Meng H, O'Connor DP, Lee B-C, Layne CS, Gorniak SL. Alterations in overground walking patterns in obese and overweight adults. Gait Posture 2017;53:145–50. <u>https://doi.org/10.1016/j.gaitpost.2017.01.019</u>.
- [42] Błaszczyk JW, Cieślinska-Świder J, Plewa M, Zahorska-Markiewicz B, Markiewicz A. Effects of excessive body weight on postural control. J Biomech 2009;42(9):1295–12300. https://doi.org/10.1016/j.jbiomech.2009.03.006.
- [43] Hue O, Simoneau M, Marcotte J, Berrigan F, Doré J, Marceau P, et al. Body weight is a strong predictor of postural stability. Gait Posture 2007;26(1):32– 8. https://doi.org/10.1016/j.gaitpost.2006.07.005.
- [44] Dutil M, Handrigan GA, Corbeil P, Cantin V, Simoneau M, Teasdale N, et al. The impact of obesity on balance control in community-dwelling older women. Age 2013;35(3):883–90. <u>https://doi.org/10.1007/s11357-012-9386-x</u>.
- [45] Rezaeipour M, Apanasenko GL. Effects of overweight and obesity on postural stability of aging females. Middle East J Rehabil Health 2018;5(4). <u>https:// doi.org/10.5812/mejrh.81617</u>.
- [46] Gribble P. The star excursion balance test as a measurement tool. Athletic Ther Today 2003;8(2):46–7.
- [47] Irez GB. The relationship with balance, foot posture, and foot size in school of Physical Education and Sports Students. Educ Res Rev 2014;9(16):551–4. <u>https://doi.org/10.5897/ERR2014.1790.</u>
- [48] Birinci T, Demirbas SB. Relationship between the mobility of medial longitudinal arch and postural control. Acta Orthop Traumatol Turc 2017;51(3):233– 7. https://doi.org/10.1016/j.aott.2016.11.004.
- [49] Alonso AC, Peterson M, Duganieri MR, Garcez-Leme LE, Mochizuki L, Bocalini DS, et al. The effects of foot morphology and anthropometry on unipodal postural control. Motriz 2016;22(1):94–8. <u>https://doi.org/10.1590/</u> S1980-65742016000100013.
- [50] Kodithuwakku Arachchige SNK, Chander H, Knight A. Flatfeet: biomechanical implications, assessment and management. Foot 2019;38:81–5. <u>https:// doi.org/10.1016/j.foot.2019.02.004</u>.
- [51] Kim J-a, Lim O-b, Yi C-h. Difference in static and dynamic stability between flexible flatfeet and neutral feet. Gait Posture 2015;41(2):546–50. <u>https:// doi.org/10.1016/j.gaitpost.2014.12.012</u>.