



# Tube Voltage, DNA Double-Strand Breaks, and Image Quality in Coronary CT Angiography

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**Objective:** To evaluate the effects of tube voltage on image quality in coronary CT angiography (CCTA), the estimated radiation dose, and DNA double-strand breaks (DSBs) in peripheral blood lymphocytes to optimize the use of CCTA in the era of low radiation doses.

**Materials and Methods:** This study included 240 patients who were divided into 2 groups according to the DNA DSB analysis methods, i.e., immunofluorescence microscopy and flow cytometry. Each group was subdivided into 4 subgroups: those receiving CCTA only with different tube voltages of 120, 100, 80, or 70 kVp. Objective and subjective image quality was evaluated by analysis of variance. Radiation dosages were also recorded and compared.

**Results:** There was no significant difference in demographic characteristics between the 2 groups and 4 subgroups in each group (all  $p > 0.05$ ). As tube voltage decreased, both image quality and radiation dose decreased gradually and significantly. After CCTA,  $\gamma$ -H2AX foci and mean fluorescence intensity in the 120-, 100-, 80-, and 70-kVp groups increased by 0.14, 0.09, 0.07, and 0.06 foci per cell and 21.26, 9.13, 8.10, and 7.13 (all  $p < 0.05$ ), respectively. The increase in the DNA DSB level in the 120-kVp group was higher than those in the other 3 groups (all  $p < 0.05$ ), while there was no significant difference in the DSBs levels among these latter groups (all  $p > 0.05$ ).

**Conclusion:** The 100-kVp tube voltage may be optimal for CCTA when weighing DNA DSBs against the estimated radiation dose and image quality, with further reductions in tube voltage being unnecessary for CCTA.

**Keywords:** Radiation dosage; Computed tomography angiography; Immunofluorescence microscopy; Flow cytometry; DNA damage

## INTRODUCTION

Coronary CT angiography (CCTA) has been widely used for diagnosing coronary artery disease, but the radiation dose in CCTA should not be underestimated (1-3). At present, various techniques for reducing radiation dose have been developed, such as prospective electrocardiogram (ECG) triggering, reduction in tube voltage, and iterative reconstruction

(IR) (4-10). Since the radiation dose is proportional to the square of the tube voltage, reducing tube voltage is the most effective method to reduce radiation dose. A tube voltage of 70 kVp in CCTA has been reported to be feasible for obtaining high diagnostic accuracy (10); however, this approach is mostly restricted to subjects with a body mass index (BMI) less than 25 kg/m<sup>2</sup> to ensure diagnostic image quality. A reduction in the tube voltage can result in

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deterioration of image quality and subsequent limitations in clinical use, and even an increase in the scattered X-rays absorbed by the subjects. Thus, although minimizing radiation dosage is an overarching goal in any form of diagnostic radiology, in the realm of CCTA, it can eventually result in loss of clinical utility, and hence it is unreasonable to pursue the lowest estimated radiation dose in every case.

In clinical practice, physical measurements such as effective dose, volumetric CT dose index (CTDI<sub>vol</sub>), and dose-length product (DLP) have been routinely used to describe the radiation doses received by subjects, but these metrics cannot reflect the interaction of X-rays with human tissue. Unlike these parameters, biological indicators could be more effective in assessing the true effect of ionizing radiation on human tissue. DNA double-strand breaks (DSBs) have been shown to be the most severe form of cellular damage produced by radiation damage (11). Immunofluorescence microscopy using probes against  $\gamma$ -H2AX, a marker of DNA DSBs, has been used to detect DSBs with much higher sensitivity than cytogenetic analysis of dicentric chromosomes (1 mGy vs. 100 mGy) (12-15). Furthermore, analysis of the mean fluorescence intensities (MFIs) of  $\gamma$ -H2AX using flow cytometry has been shown to be more objective and was used in many studies (16-18). In addition to  $\gamma$ -H2AX, other markers of DNA damage such as ataxia telangiectasia-mutated protein and P53 protein (19) can be used to detect DNA damage, but these markers are not used widely.

Biological effects have not been adequately analyzed in the assessment of radiation reduction strategies currently employed in clinical practice. The first study to assess the influence of CCTA scanning parameters on the biological effects of X-rays was published in 2010, which found that the DSB levels in patients examined with 100 kVp were approximately 30% lower than in patients examined with 120 kVp (20). However, another study reported (21) that lower tube voltage could increase DNA DSBs when the tube current is elevated. To the best of our knowledge, no study has yet attempted to optimize tube voltage and image quality from the perspective of the biological effects in CCTA studies.

Thus, the purpose of this study was to evaluate the effects of tube voltage on the image quality of CCTA, estimated radiation dose, and DSBs in peripheral blood lymphocytes, in order to optimize the use of CCTA in the era of low radiation doses.

## MATERIALS AND METHODS

### Patients

The study was approved by the local ethics committee, and written informed patient consent was obtained from each subject. Altogether 240 patients with suspected coronary artery disease were included in the study. The enrollment criteria were as follows: age greater than 18 years, BMI less than 25 kg/m<sup>2</sup>, absence of lymphoma or leukemia, no radiation therapy or chemotherapy within 6 months prior to this study, no examinations using X-rays or nuclear medicine studies within 1 week prior to this study, no contraindications to iodinated contrast agents (such as hyperthyroidism and heart failure), and no history of coronary artery bypass grafting or coronary artery stent implantation.

The patients were divided into four groups based on tube voltages used during CCTA, i.e., 120 kVp (A group), 100 kVp (B group), 80 kVp (C group), and 70 kVp (D group). Each group was further divided into 2 subgroups by random number generation. Patients in group A1–D1 underwent immunofluorescence microscopy for DNA DSB analysis, while the patients in Group A2–D2 underwent flow cytometric analysis. Except for different tube voltages, other scanning parameters were kept the same for the patients in all subgroups.

### CCTA Scan and Estimation of Radiation Dose

CCTA examination was performed in end-inspiratory breath-hold with heart rate monitoring by a prospective ECG-triggered sequence on a second-generation dual-source CT scanner (SOMATOM<sup>®</sup> Definition Flash, Siemens Healthineers, Forchheim, Germany) after intravenous administration of 60 mL of iopromide (Ultravist<sup>®</sup>, Bayer AG, Berlin, Germany) with a concentration of 370 mg of iodine/mL at 5 mL/s. Automated bolus triggering was used to determine the delay time of the arterial phase. The area of interest was placed in the aorta with an automated trigger threshold of 100 Hounsfield units (HU). Tube voltages were 120, 100, 80, and 70 kVp, respectively. The remaining scanning parameters were consistent: effective tube current, 280 mAs; rotation time = 0.28 seconds; collimation = 0.6 mm x 128. The scanning range was from the tracheal carina to the bottom of the heart. Sinogram affirmed iterative reconstruction (SAFIRE; Siemens Healthineers, Forchheim, Germany, strength level of 3) was used per default. Raw data were transferred to a clinical

workstation for image postprocessing.

The CTDIvol and DLP were recorded for each CCTA study according to the patient's study protocol report. Effective dose was estimated by multiplying the DLP by a conversion factor of 0.014 mSv/mGy·cm (22).

### Blood Sampling

Two milliliters of whole venous blood were taken from the antecubital vein before and 20 minutes after the examination, respectively. After dilution with phosphate-buffered saline (PBS), peripheral blood mononuclear cells (PBMCs) were obtained by Ficoll density-gradient centrifugation and the samples were washed twice with PBS.

### Immunocytochemical Staining and Fluorescence Microscopy

The lymphocytes of groups A1, B1, C1, and D1 were resuspended in 2 mL of 1640 medium. Then, 30- $\mu$ L samples were placed on each cover glass and incubated at room temperature for about 1 hour. The cells were then fixed with 200  $\mu$ L of 4% paraformaldehyde for 20 minutes, and permeabilized with 0.3% Triton X-100 PBS for 10 minutes at room temperature. After being blocked with sheep serum albumin for 30 minutes at room temperature, the samples were incubated with rabbit anti- $\gamma$ H2AX antibody (clone JBW301, Upstate, Chandlers Ford, UK) overnight and with mouse anti-rabbit secondary antibodies (Invitrogen, Paisley, UK) for 1 hour. Finally, the samples were stained using UltraCruz<sup>TM</sup> (Santa Cruz, CA, USA, containing 4, 6-diamidino-2-phenylindole) and mounted with neutral resin. Fluorescence images were obtained by using an Olympus IX71 inverted fluorescence microscope (Olympus Co., Tokyo, Japan). For the quantitative analysis, red fluorescent foci (Supplementary Fig. 1) were counted in 200 cells to account via background correction. The number of foci in 200 cells was measured and averaged. Analysis of foci in PBMCs was performed in only those cells with lymphocyte-like morphology. The number of X-ray-induced  $\gamma$ -H2AX foci was obtained by subtracting the number of  $\gamma$ -H2AX foci of the samples obtained just before and 20 minutes after the CCTA.

### Flow Cytometry and Mean of Fluorescence Intensity

The lymphocytes in groups A2, B2, C2, and D2 were diluted to  $1 \times 10^6$  cells/mL with 1640 medium, fixed with 4% paraformaldehyde at room temperature for 15 minutes, and permeabilized with 0.1% Triton X-100 for 10 minutes.

The samples were washed with PBS 3 times after each step. Samples were incubated with FITC-CD3 antibody (BD Biosciences, Franklin Lakes, NJ, USA) and APC- $\gamma$ -H2AX antibody (BD Biosciences) for 30 minutes protected from light. The samples were then analyzed by a flow cytometer (BD Calibur, BD Bioscience). Based on forward and side light scattering, PBMCs were gated for viable single-cell events. MFI of  $\gamma$ -H2AX in positive T-lymphocytes was evaluated using FlowJo software (V10.0.2, Tree Star, Inc., Ashland, OR, USA) (Supplementary Fig. 2).

### Objective and Subjective Image Quality Evaluations

Image quality was objectively evaluated by measuring the average CT value in HU and image noise by the standard deviation (SD) in circular regions of interest (ROIs). These measurements were performed in the right coronary artery (RCA), left anterior descending artery (LAD), left circumflex artery (LCX), aorta, and sternocleidomastoid muscle. The ROIs were either circular or ellipsoidal and covered the maximum region of the vessel, excluding walls, plaques, and calcium regions. ROIs within coronary arteries and muscle tissue had an area of 5–10 mm<sup>2</sup>, while ROIs within the aorta were 10 cm<sup>2</sup> in area (Supplementary Fig. 3). The signal-to-noise ratio (SNR) was calculated as the ratio between the mean CT value and the SD, while contrast-to-noise ratio (CNR) was calculated as  $(\text{mean CT value}_{\text{organ of interest}} - \text{mean CT value}_{\text{muscle}}) / \text{SD}_{\text{heart muscle}}$ .

Two independent blinded observers (with five- and three-year experience in CCTA, respectively) scored the overall image quality using a 5-point scale (Supplementary Fig. 4), where 5 = excellent; 4 = above average; 3 = acceptable; 2 = suboptimal, but images are still interpretable; and 1 = very poor (nondiagnostic). Image noise was assessed as follows: 5 = minimal noise; 4 = less than average; 3 = average; 2 = higher than average; 1 = unacceptably high (23). In case of disagreement between the two observers, consensus was reached in a joint reading to determine the final image quality score.

### Statistical Analysis

Data in this study were analyzed using Statistical Product and Service Solutions (SPSS) software (version 19, IBM Corp., Armonk, NY, USA). Shapiro–Wilk testing was applied to analyze normal distribution of data sets. Normally distributed variables were expressed as mean  $\pm$  SD values, and non-normally distributed variables were displayed as median with interquartile ranges. Sex was compared by

chi-squared test, and other demographic characteristics and radiation dose between groups were compared using independent sample *t* test and one-way analysis of variance, if appropriate. Wilcoxon signed-rank test was used for DNA DSBs before and after CCTA, and Kruskal-Wallis rank sum test was used for comparison of  $\gamma$ -H2AX foci and MFI among groups. Analysis of variance was performed to compare the objective measurements (CT value, SNR, and CNR) of the standard in four subgroups. Interobserver variability between the 2 observers with regard to subjective image quality assessment was evaluated with  $\kappa$  statistics ( $\kappa < 0.20$ , poor agreement;  $0.21 < \kappa < 0.40$ , fair agreement;  $0.41 < \kappa < 0.60$ , moderate agreement;  $0.61 < \kappa < 0.80$ , good agreement;  $0.81 < \kappa < 1.00$ , very good agreement).  $P < 0.05$  was considered statistically significant.

## RESULTS

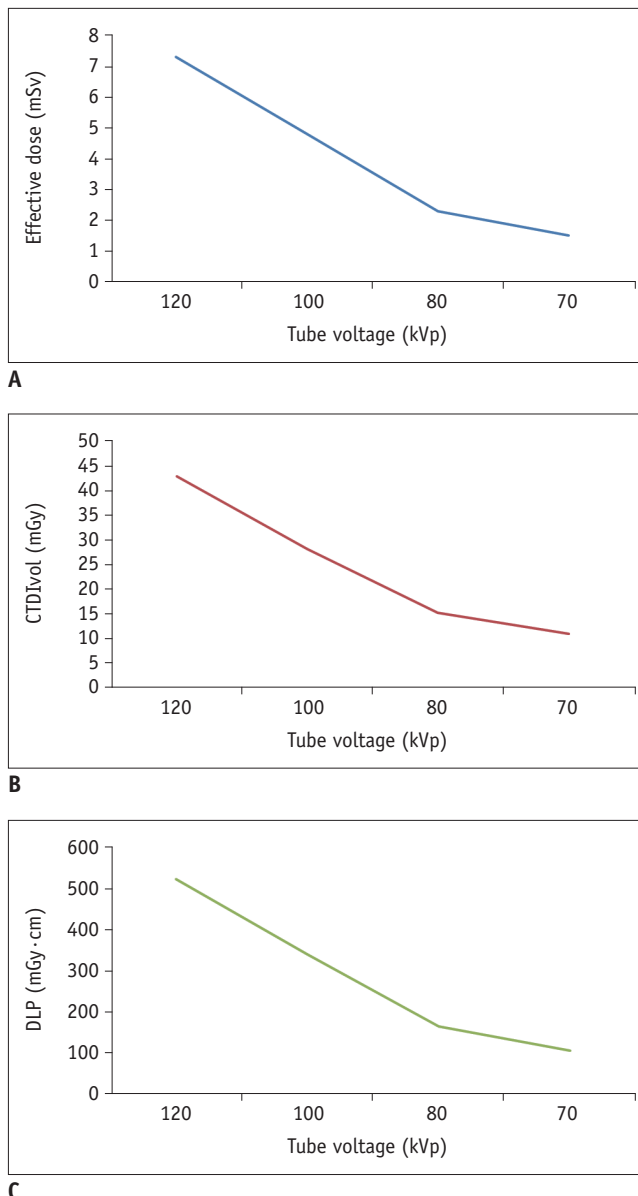
### Demographic Characteristics and Radiation Dose

The distribution of demographic data among groups is shown in Table 1. There were no significant differences in demographic characteristics among the four subgroups (subgroup A1, B1, C1, D1 and subgroup A2, B2, C2, D2) (all  $p > 0.05$ ). As the tube voltage decreased, the estimated radiation dose (effective dose, CTDIvol, and DLP) decreased as well (all  $p < 0.001$ ) (Fig. 1). Table 2 shows the radiation doses in different tube voltage groups.

### $\gamma$ -H2AX Yield after CCTA

#### $\gamma$ -H2AX Foci Level

The median baseline levels of  $\gamma$ -H2AX foci were 0.24 (0.16, 0.33) foci/cell in subgroup A1, 0.20 (0.18, 0.23) foci/cell in subgroup B1, 0.28 (0.18, 0.23) foci/cell in subgroup C1, and 0.21 (0.17, 0.27) foci/cell in subgroup D1. There was no significant difference in the baseline levels of  $\gamma$ -H2AX



**Fig. 1. Estimated radiation dose trends over different tube voltages.**

As tube voltage decreases, estimated radiation dose (effective dose (A), CTDIvol (B), and DLP (C)) decreases. CTDIvol = volumetric CT dose index, DLP = dose-length product

**Table 1. Demographic Characteristics and Estimated Radiation Doses among Subgroups**

Parameters	Immunofluorescence Staining				P	Flow Cytometry				P
	A1	B1	C1	D1		A2	B2	C2	D2	
Sex, number					0.199					0.750
Male	22	19	19	14		16	19	16	15	
Female	8	11	11	16		14	11	14	15	
Age, years	53 ± 13	56 ± 12	56 ± 12	54 ± 12	0.243	56 ± 10	59 ± 11	59 ± 11	55 ± 11	0.320
Height, cm	169.5 ± 5.7	167.6 ± 8.9	169.3 ± 6.2	167.2 ± 6.8	0.453	167.0 ± 7.2	167.3 ± 8.7	167.0 ± 7.0	166.5 ± 8.0	0.985
Weight, kg	68.4 ± 6.5	66.5 ± 9.3	69.3 ± 5.2	66.8 ± 6.8	0.363	66.1 ± 7.6	66.9 ± 8.3	66.6 ± 6.4	64.1 ± 13.1	0.623
BMI, kg/m <sup>2</sup>	23.7 ± 1.1	23.5 ± 1.5	24.2 ± 0.8	23.8 ± 1.0	0.189	23.6 ± 1.2	23.8 ± 1.0	23.8 ± 0.9	23.0 ± 3.8	0.363

A = 120 kVp group, B = 100 kVp group, BMI = body mass index, C = 80 kVp group, D = 70 kVp group

**Table 2. Radiation Doses at Different Tube Voltages**

Groups	Effective dose, mSv	CTDIvol, mGy	DLP, mGy·cm
120 kVp (n = 60)	7.3 ± 1.8	42.9 ± 7.7	523.3 ± 130.1
100 kVp (n = 60)	4.8 ± 0.7	28.2 ± 4.4	339.7 ± 47.2
80 kVp (n = 60)	2.3 ± 0.4	15.3 ± 2.8	163.9 ± 27.9
70 kVp (n = 60)	1.5 ± 0.2	11.0 ± 2.7	105.0 ± 16.7
<i>p</i> value	< 0.001	< 0.001	< 0.001

Values are mean ± standard deviation. CTDIvol = volumetric CT dose index, DLP = dose-length product

foci among the four subgroups ( $p = 0.066$ ). However,  $\gamma$ -H2AX foci in the four subgroups increased significantly by 0.14, 0.09, 0.07, and 0.06 foci/cell after CCTA (all  $p < 0.05$ ) in comparison with the baseline (Fig. 2).

### MFI of $\gamma$ -H2AX

The median baseline levels of  $\gamma$ -H2AX MFI were 71.1 (56.3, 129.0) in subgroup A2, 83.2 (67.7, 135.0) in subgroup B2, 93.2 (65.8, 121.1) in subgroup C2, and 88.2 (68.5, 235.2) in subgroup D2. There was no significant difference in the baseline levels of  $\gamma$ -H2AX MFI among the four subgroups ( $p = 0.196$ ). However, radiation-induced  $\gamma$ -H2AX MFI increased significantly by 21.26, 9.13, 8.10, 7.13 after CCTA in all four subgroups (all  $p < 0.05$ ) (Fig. 3).

### Comparisons among Groups

#### $\gamma$ -H2AX Foci Level

Figure 4A shows the changes in  $\gamma$ -H2AX foci levels after CCTA in subgroups A1, B1, C1, and D1, respectively. As tube voltage decreased, the increment in  $\gamma$ -H2AX foci decreased gradually ( $p = 0.001$ ). Post-hoc analysis showed that the change in  $\gamma$ -H2AX foci levels in subgroup A1 was higher than those in the other three subgroups (B1, C1, D1) after CCTA ( $p = 0.003$ ,  $p = 0.006$ ,  $p < 0.001$ , respectively), but significant differences were not observed among the three subgroups ( $p = 0.184$ ).

#### MFI of $\gamma$ -H2AX

Figure 4B shows the changes in  $\gamma$ -H2AX MFI levels after CCTA in subgroups A2, B2, C2, and D2. These findings corroborated those found via immunofluorescence microscopy. Namely, as tube voltage decreased, the increment in  $\gamma$ -H2AX MFI decreased gradually ( $p < 0.001$ ), but no significant difference was observed among subgroups B2, C2, and D2 ( $p = 0.126$ ), while the change in  $\gamma$ -H2AX MFI in subgroup A2 was found to be higher than those in

the other three subgroups B2, C2, and D2 ( $p = 0.001$ ,  $p = 0.001$ , and  $p < 0.001$ , respectively).

### Objective and Subjective Image Quality Comparisons

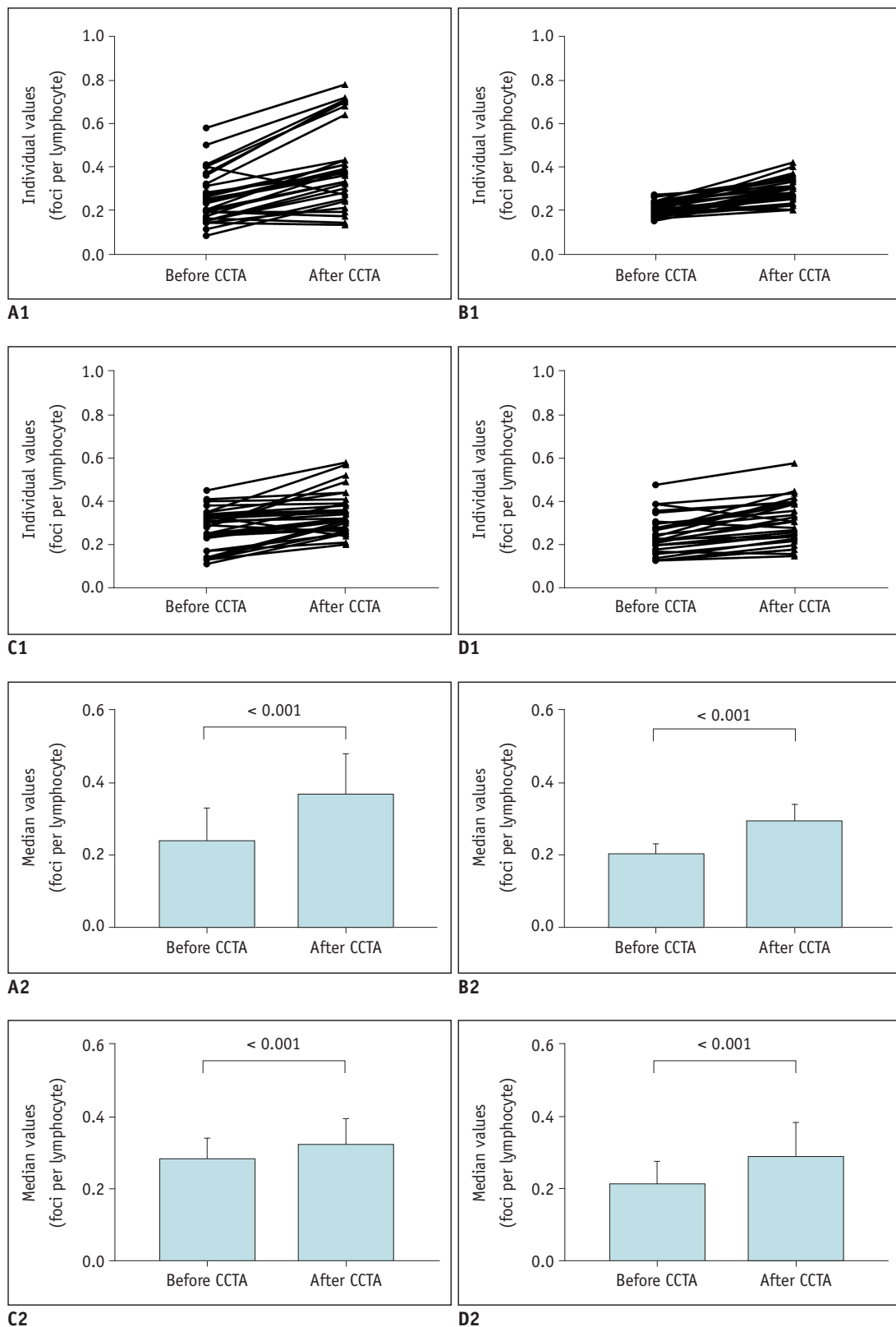
Supplementary Table 1 provides the results of objective image quality evaluations. The CT values in the 120-kVp group were lower and the SNRs of the RCA, LAD, LCX, and aorta were significantly higher than those in the other three subgroups (all  $p < 0.001$ ) (Fig. 5). However, there were no significant differences in the CNRs of the RCA, LAD, LCX, and aorta among the 120-, 100-, and 80-kVp subgroups ( $p = 0.094$ ,  $p = 0.122$ ,  $p = 0.128$ , and  $p = 0.143$ , respectively). The image noise was the highest in the 70-kVp group ( $p = 0.012$ ).

As tube voltage decreased from 120 kVp to 70 kVp, the scores for overall image quality decreased and those for noise increased significantly (all  $p < 0.001$ ). No study at any tube voltage was scored lower than 3, but the ratio of score 5 for image quality and noise decreased as tube voltage decreased (Fig. 6). Interobserver agreement was good to fair for 120 kVp ( $\kappa = 0.704$ ), 100 kVp ( $\kappa = 0.647$ ), 80 kVp ( $\kappa = 0.379$ ), and 70 kVp ( $\kappa = 0.288$ ). The interobserver agreements were significantly different among the four subgroups ( $p < 0.001$ ).

### DISCUSSION

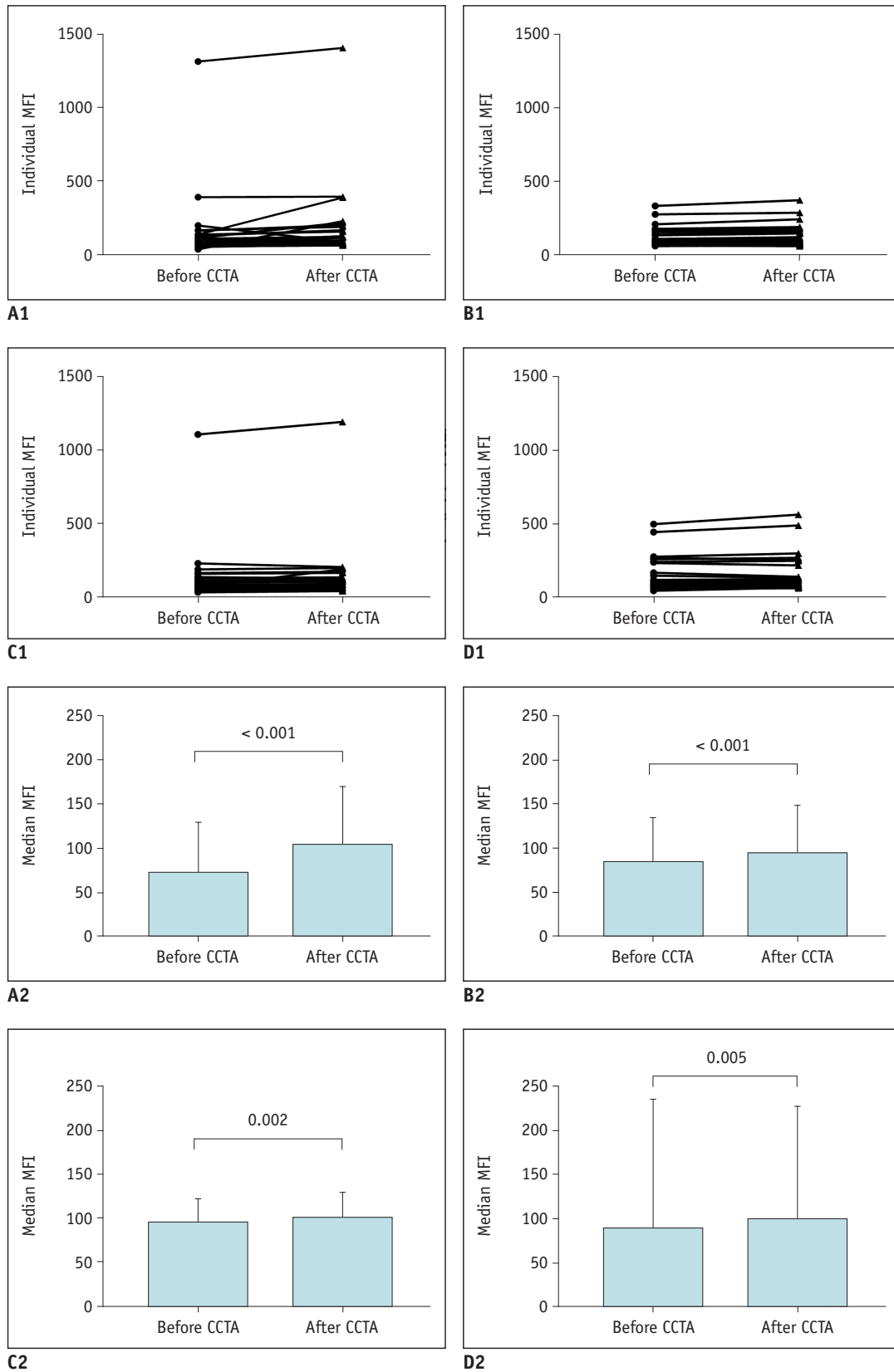
This study found that DNA DSBs reached a plateau when weighed against image quality and radiation dose, as the tube voltage decreased from 120 kVp to 100 kVp, which indicates that 100 kVp may be optimal for CCTA studies on the basis of biological effects.

For many years, CCTA studies assessing radiation dosage focused on image quality for assessment of different radiation dose reduction methods. As reported, with IR techniques, a lower tube voltage or current would decrease the estimated effective radiation dose. Thus, the most effective method to reduce radiation dose, which involves the use of lower tube voltages such as 70 kVp, has been used for CCTA studies (24, 25). We have confirmed that excessive reductions in tube voltage harbor the risk of sacrificing image quality (CT values, SNR, and CNR), as reported in other studies (24, 26). However, the image quality of all included CCTA images still satisfied diagnostic requirements because the BMI of all included patients was set at less than 25 kg/m<sup>2</sup>, and the dosage of contrast medium at the lower tube voltage was kept the same as



**Fig. 2. DNA DSBs before and after CCTA by immunofluorescence microscopy.**

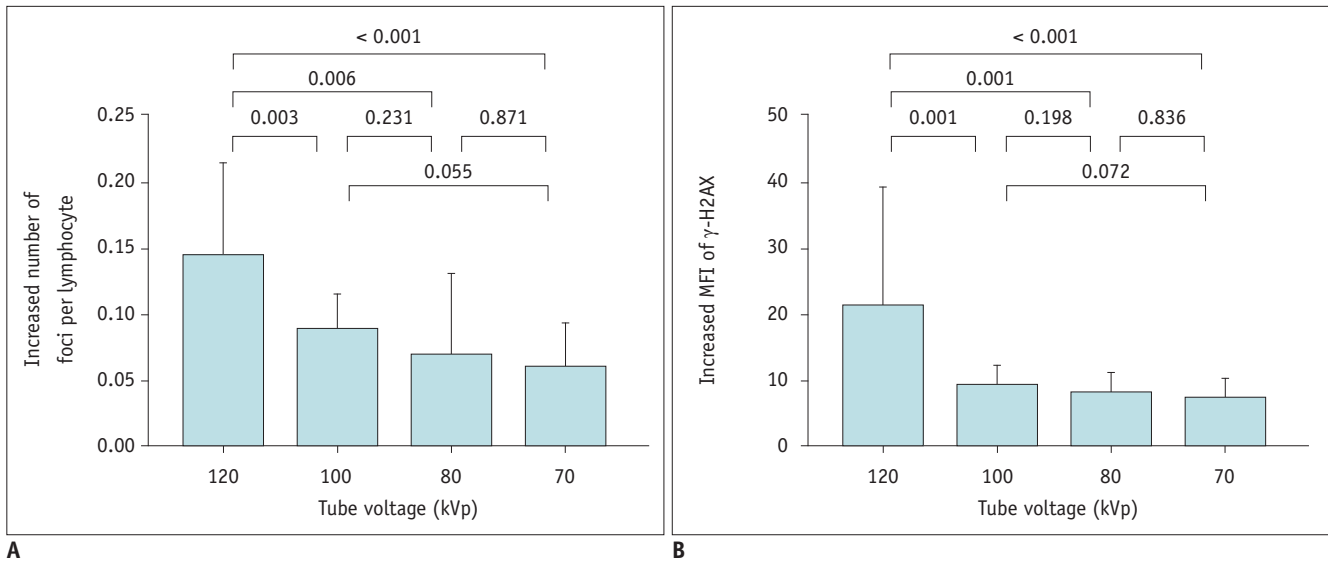
After CCTA, immunofluorescence microscopy shows significant increase in  $\gamma$ -H2AX foci per lymphocyte in subgroups examined with 120 kVp (A1, A2), 100 kVp (B1, B2), 80 kVp (C1, C2), and 70 kVp (D1, D2). Bars indicate median values with median absolute deviation (A2-D2) and individual values are interconnected with line (A1-D1). CCTA = coronary CT angiography, DSB = double-strand break



**Fig. 3. DNA DSBs before and after CCTA by flow cytometry.** Individual MFI and median MFI is increased significantly after CCTA (A2-D2) in subgroups examined with 120 kVp (A1, A2), 100 kVp (B1, B2), 80 kVp (C1, C2), and 70 kVp (D1, D2). Individual values are interconnected with line (A1-D1). MFI = mean fluorescence intensity

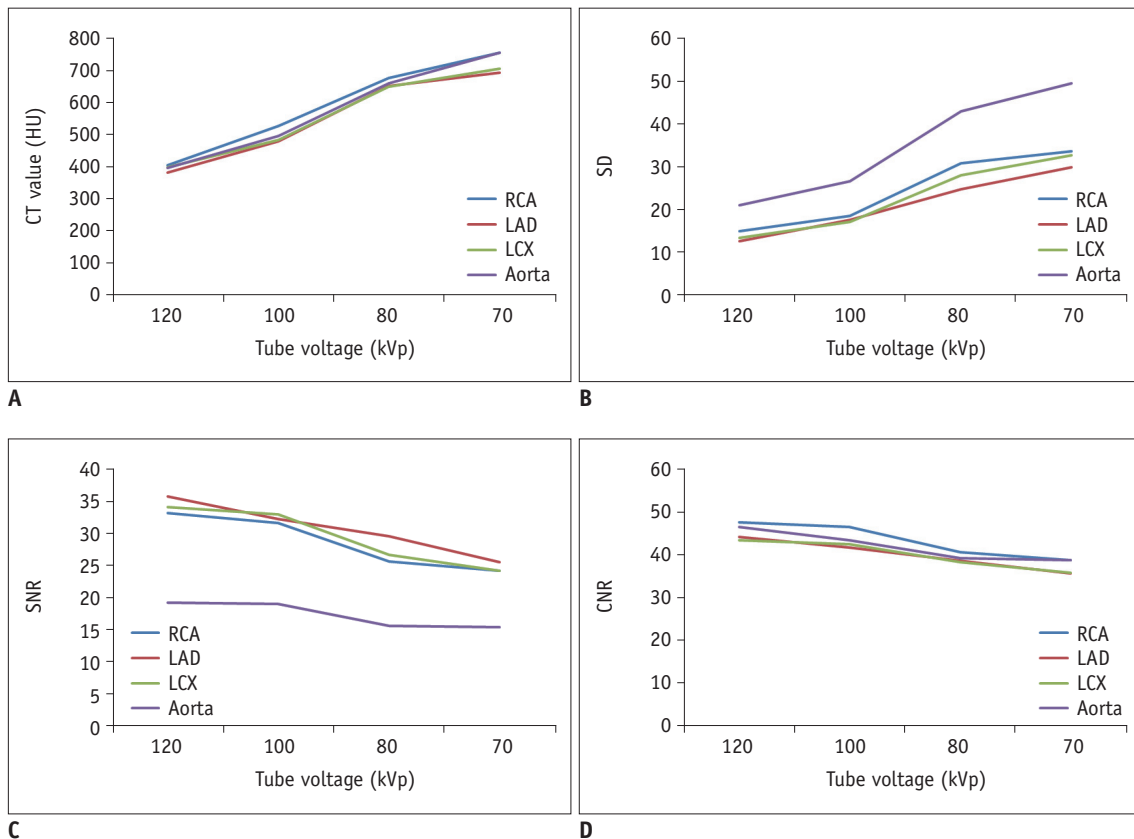
that at higher tube voltages, which may have contributed to the overall diagnostic quality of CCTA acquisitions in this study.

The relationship between radiation dose and DNA damage has recently become a topic of intense research. The levels of DNA DSBs in peripheral blood lymphocytes are reported



**Fig. 4. Changes in  $\gamma$ -H2AX foci and MFI levels after CCTA examination.**

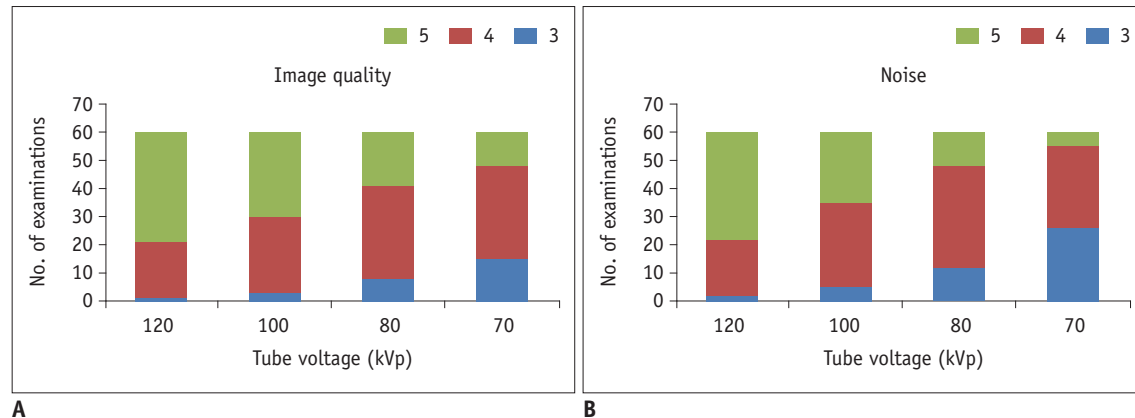
**A, B.** Panels show changes in DNA DSBs as tube voltage decreased. There are no significant differences in DNA DSBs among 100-, 80-, and 70-kVp subgroups ( $p = 0.184, 0.126$ ). DNA DSB level at 120 kVp is higher than those in other three subgroups (all  $p < 0.05$ ) are.



**Fig. 5. Objective image quality in different tube voltage groups.**

CT values **(A)** and noise **(B)** of RCA, LAD, LCX, and aorta increased gradually when tube voltage decreased, while SNR **(C)** and CNR **(D)** decreased. CNR = contrast-to-noise ratio, LAD = left anterior descending artery, LCX = left circumflex artery, RCA = right coronary artery, SD = standard deviation, SNR = signal-to-noise ratio





**Fig. 6. Image quality and noise distribution in different tube voltage groups.** No CCTA study at any tube voltage group scored less than 3 points in image quality (A) and noise (B). However, ratio of 5-point examinations increased as tube voltage increased in both of image quality and noise.

to be related to the radiation dose (27, 28). Zhang et al. (21) reported that a lower tube voltage (80 kVp) caused more severe DNA DSBs than a higher tube voltage (140 kVp), which suggested that reducing tube voltage may actually be harmful because of the increased scattered radiation absorbed by the body. However, in the current study, the increase in the levels of DNA DSBs after CCTA at 100, 80, and 70 kVp showed no statistical difference, a finding supported by the results reported by Brand et al. (29). There was a significant decline in the estimated radiation dose and image quality as the tube voltage decreased, but DNA DSB levels remained stable although tube voltage decreased from 100 kVp to 70 kVp. These results suggest that the effect of lower radiation doses (< 5 mSv) on DNA DSBs was very minimal. Thus, a biological effect-based approach may be more relevant in weighing ionizing radiation damage and image quality than an estimated radiation dose strategy.

In our study, we used both immunofluorescence staining and flow cytometry to assess the relationships among DNA damage, estimated radiation dose, and image quality (19). The results showed that when tube voltage was reduced from 120 kVp to 100 kVp, the DNA DSB level reduced by 30%, which was previously reported by immunofluorescence microscopy (20) and was also supported by a similar reduction observed by immunofluorescence (39%). Although immunofluorescence microscopy has been reported to show much higher sensitivity, flow cytometry had sufficient analytical sensitivity to measure the levels of DNA damage due to the large number of cells analyzed in clinical practice, as noted by Johansson et al. (18). Therefore, both methods could be used based on the laboratory conditions.

We acknowledge certain limitations with this study. First,

the sample size in the subgroups was small, and a larger population will be needed in future studies to validate our findings further. Second, although we used two methods to demonstrate the same results for the quantification of DNA DSBs, they were not used simultaneously in the same patient population. Additionally, other detection methods could be used for DNA DSBs in future studies. Third, the effect of the contrast medium on DNA DSBs was not investigated because this was not a variable designated to be optimized with respect to tube voltage at the outset of the study. Fourth, different radiation doses resulting from different tube voltages may affect our observed results. Except tube voltage, all remaining scan parameters were kept constant in our study. Thus, the interaction of tube voltage and radiation dose on DNA DSBs needs to be studied further. Finally, we did not compare the technique used herein with digital subtraction angiography or other gold standards. However, Lee et al. (30) have shown that tube voltage does not affect the accuracy of stenosis measurement based on a phantom study.

In conclusion, this study indicates that a biological effect-based approach is rational to weigh radiation damage against image quality. A 100-kVp tube voltage may be optimal for CCTA studies if DNA DSBs are weighted, rather than estimated effective radiation dose, vis-a-vis image quality.

### Supplementary Materials

The Data Supplement is available with this article at <https://doi.org/10.3348/kjr.2019.0932>.

### Conflicts of Interest

UJS is a consultant for and/or receives research support from Astellas, Bayer, Elucid BioImaging, General Electric, Guerbet, HeartFlow, and Siemens Healthineers. The other authors have no conflicts of interest to disclose.

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